

# Applying the Difference Term Approach for Low Frequency Biomedical Filter

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#### Abstract

Low frequency continuous time filters are essential analog blocks for biomedical applications. Integrating such filters having large time constants is difficult as it requires large component values. A novel approach to scale down the pole frequency is presented. A 5-bit reduction in the cut off frequency is achieved. This is made possible through adding a passive resistor in the forward path of the op-amp based integrator introducing a difference term of the pole frequency. Also, the filter topology is modified to avoid changing the quality factor. As an example, a 2<sup>nd</sup> order low pass filter is designed and simulated. Simulation results show that the pole frequency is scaled down from 1.43 MHz to 4.97 kHz while maintaining tuning of 30% around the nominal value by controlling only one resistor.

#### Introduction

Very low frequency filters has wide range of applications in biomedical signal processing [1-6]. The bandwidth of Electroencephalogram (EEG), for example, refers to the monitored signal due to the brain activities and Electrocardiogram (ECG) which is a test for the electrical activities that being recorded due to the heart beat's, is 0.1-30 Hz and 0.01-100 Hz, respectively. The amplitude and frequency ranges of some physiological signals are depicted in Figure 1 [7].

Amplification and pre-filtering of these signals are mandatory before further digital signal processing (DSP). However, such very low frequency filters needs large passive components values which cannot be implemented in standard analog integrated circuit (IC) fabrication. Typical values for integrated resistors are from several ohms to  $40k\Omega$  and for capacitors are from 0.5 pF to 50 pF [7]. This has been a challenging design problem due to the difficulty in developing efficient methods to achieve large time constant using integrated passive elements. This paper presents a new CMOS circuit technique for implementing a very low frequency Active-RC based filters by applying a difference term approach which has been used for realizing very low frequency oscillator. The following section presents the methodology of the proposed technique. Simulation results are given below.



### **Proposed Approach**

The transfer function of the low pass filter is given in the following equation:

$$\frac{V_0}{Vin} = \frac{K}{S^2 + \left(\frac{Q}{BW}\right)S + \omega^2}$$
(1)

where K is the gain of the filter, Q is the quality factor, BW represents the bandwidth and  $\omega$  is the corner frequency (3-dB frequency). The corner frequency of the low pass is given by:

$$f = \left(\frac{1}{2\pi CR}\right) \tag{2}$$

Obviously to get low frequencies in the range of few hertz to few kilo-hertz, large capacitors and resistors are needed. One novel approach to scale down the frequency is to introduce a difference term of R1and R2,  $m=R_1-R_2$ , in  $\omega$  term. So, as m decreases the frequency scaled down and very low corner frequency can be obtained. This approach has been used for realizing very low frequency oscillators 'VLFO' [8-10]. The challenge in this approach in filter design is to introduce difference term m, not only in the pole frequency  $\omega$ , but also in the s-coefficient term,  $\left(\frac{Q}{BW}\right)$ , to cancel the effect of m in Q and hence the quality factor can be controlled via ratio of resisters  $\frac{R_s}{R_y}$  independent of  $R_1-R_2$ . So the filter topology is adjusted to tackle this problem by introducing a square of the difference term m<sup>2</sup> in the pole

problem by introducing a square of the difference term  $m^2$ , in the pole frequency and m in the s-coefficient term and hence the effect of m on the Q is cancelled. Also  $m^2$  is introduced in the numerator coefficient such that the gain is not disturbed.

A low pass filter can be obtained using the integrator shown in

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(Figure 2) in two integrator loop topology. The transfer function of this filter shown in (Figure 3) is obtained as follows:

$$\frac{V_0}{V_{in}} = \frac{\frac{R_f(R_1 - R_2)(R_3 - R_4)}{C_1 C_2 R_1 R_2 R_3 R_4 R_{in}}}{S^2 + S\left(\frac{R_f(R_1 - R_2)}{C_2 R_1 R_2 R_G}\right) + \frac{R_f(R_1 - R_2)(R_3 - R_4)}{C_1 C_2 R_1 R_2 R_3 R_4 R_5}}$$
(3)

From the above transfer function and assuming  $R_f = R_5 = R$ ,  $R_1 = R_3$ ,  $R_2 = R_4$  and  $C_1 = C_2 = C$ , we can obtain the DC gain, the corner frequency and the quality factor as follows:

$$DCGain = \frac{R}{R_{in}}, Q = \frac{R_G}{R}, 2\pi f = \frac{(R_1 - R_2)}{CR_1R_2}$$
(4-6)

In this topology, it can be seen clearly that the DC gain, the quality factor and the corner frequency can be all controlled independently (Equation 4-Equation 6). Moreover, the corner frequency can be scaled down exploiting the presence of the difference term of resistors in the numerator. However, this technique suffers from the high sensitivity (Equation 8). The sensitivity for the proposed filter is given below:

$$S_{R_{1}}^{Q} = S_{R_{2}}^{Q} = S_{\omega}^{Q} = 0, \ S_{Rg}^{Q} = -S_{R}^{Q} = -S_{DCGain}^{Q} = 1$$
(7)

$$S_{R1}^{\omega} = \frac{R_2}{R_1 - R_2}$$
(8)

## **Simulation Results**

SPICE Simulation tests have been done using 2<sup>nd</sup> order low pass filter (LPF) with frequency scaling technique and values of C = 100 pF, R<sub>1</sub> = 10 K $\Omega$  for different cases of R<sub>2</sub>. Using Mont Carlo analysis, the filter has been extensively simulated for 100 runs with an applied resistance tolerance of 1% to R<sub>1</sub> and R<sub>2</sub> to check the reliability of the proposed filter. The frequency responses of three different cases, namely R<sub>2</sub> = 9.4 k $\Omega$ , R<sub>2</sub> = 5 k $\Omega$  and R<sub>2</sub> = 1 k $\Omega$ , are provided in Figure 4.





Figure 5 shows the histogram of one case where a 4-bit pole frequency reduction is achieved  $R_2 = 9.4k\Omega$ , which represents the distribution of the samples developed by Monte Carlo analysis over a range of frequency. Table 1 summaries the results obtained from the conducted simulation and percentage of error.

It can be interfered from (Table 1) that this technique can be used for both directions, up scaling and down scaling. Capacitor arrays can be incorporated to introduce a 30% tuning in the pole frequency which was achieved in lately published work [11]. As a result, a 5-bit pole frequency reduction can be realized as indicated in (Table1) giving a probability of p=0.76 and a 6-bit reduction if we allow 50% tuning.

### Conclusion

A new CMOS circuit technique for implementing a very low frequency active-RC based filter by employing the difference term







$R_{2}(k\Omega)$	Number of Bit Reduction, n	Pole Fre- quency (kHz)	Deviation from Nominal value	In Range Sam- ples out of 100
1	NA	1432.4	1.33%	100
5	NA	159.155	3%	100
8.9	3 bits	19892	10%	82
9.4	4 bits	9943	20%	81
9.7	5 bits	4973	30%	76
9.85	6 bits	2489	50%	63

**Table 1:** Summary of the monte carlo simulation.

Page 3 of 3

approach is proposed. Sensitivity and independent gain, quality and pole frequency programmability is addressed. Simulation results of the filter shows a huge range of pole frequency scaling from 1.43 MHz to 4.97 KHz. These results are promising and we are working in optimization phase to meet certain specifications heading to IC fabrication. Finally, this technique can be combined with other techniques, R2R approach for example, to realize a very low pole frequency in order of 0.1 Hz.

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#### References

- 1. Li Y, Poon CY, Zhang YT (2010) Analog integrated circuits design for processing physiological signals. IEEE Rev Biomed Eng 3: 93-105.
- Wong AK, Pun K, Zhang Y, Nang Leung K (2008) 'A low-power CMOS frontend for photoplethysmographic signal acquisition with robust DC photocurrent rejection.' IEEE Tran. on Biomedical Circuits and Syst 2 280-288.
- Lee S, Cheng C (2008) 'Systematic design and modeling of a OTA-C filter for portable ECG detection.' IEEE Tran. on Biomedical Circuits and Syst 3: 53-64.
- 4. Mollazadeh M, Murari K, Cauwenberghs G, Thakor N (2009) 'Micropower

CMOS integrated low-noise amplification, filtering, and digitization of multimodal neuropotentials' IEEE Tran. on Biomedical Circuits and Syst 3: 1-10.

- Mollazadeh M, Murari K, Cauwenberghs G, Thakor N (2009) 'Wireless micropower instrumentation for multimodal acquisition of electrical and chemical neural activity' IEEE Tran. on Biomedical Circuits and Syst 3: 388-397.
- Piskorowski J (2010) 'Digital notch filter with time-varying quality factor for the reduction of powerline interference'. Circuits and Systems (ISCAS), Proceedings of 2010 IEEE International Symposium on Paris. 2706-2709.
- Webster J (1999) "Medical Instrumentation: Application and Design". CRC Press, 3<sup>rd</sup> Edition.
- Senani R, Bhasjar D (1991) 'Single Op-Amp Sinusoidal Oscillators Suitable for Generation of Very Low Frequencies', IEEE trans. on instrumentation and measurement 40: 777-779.
- Elwakil A (1998) 'Systematic Realization Low-Frequency Oscillators Using Composite Passive-Active Resistors', IEEE trans. On instrumentation and measurement 47: 584-586.
- Bhashar DR and Senani R (2006) 'New CFOA-Based Single-Element-Controlled Sinusoidal Oscillators', IEEE tran. on instrumentation and measurement 55: 2014-2021.
- Alzaher H, Tasadduq N, Mahnashi Y (2012) 'An Integrated Active-RC Powerline Notch Filter for Biopotential Acquisition Devices' International Joint Conference on Biomedical Engineering Systems and Biotechnologies, Purtogal 1<sup>st</sup>-4<sup>th</sup> Feb.